

Evaluation of Gold Nanoparticle Size Effect on Dose Enhancement Factor in Megavoltage Beam Radiotherapy Using MAGICA Polymer Gel Dosimeter

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ABSTRACT

Background: Gold nanoparticles (GNPs) are among the most promising radio-sensitive materials in radiotherapy. Studying the effective sensitizing factors such as nanoparticle size, concentration, surface features, radiation energy and cell type can help to optimize the effect and possible clinical application of GNPs in radiation therapy. In this study, the radiation sensitive polymer gel was used to investigate the dosimetric effect of GNP size in megavoltage (MV) photon beam radiotherapy.

Material and Methods: GNPs with the size of 30nm, 50nm and 100nm in diameter were used. Transmission electron microscope (TEM) and dynamic light scattering (DLS) were applied to analyze the size of nanoparticles. The MAGICA polymer gel was synthesized and impregnated with different sizes of GNPs. The samples were irradiated with 6MV photon beam and 24 hours after irradiation, they were read using a Magnetic Resonance Imaging (MRI) scanner. Macroscopic Dose Enhancement Factor (DEF) was measured to compare the effect of GNP size. The MAGICA response of the 6MV x-ray beam was verified comparing Percentage Depth Dose (PDD) curve extracted from polymer gel dosimetry and Treatment Planning System (TPS).

Results: MAGICA polymer gel dose response curve was linear in the range of 0 to 10 Gy. DEFs by adding 30nm, 50nm and 100nm GNPs were 1.1, 1.17 and 1.12, respectively. PDD curves of polymer gel dosimeter and treatment planning system were in good agreement.

Conclusion: The results indicated a substantial increase in DEF uses a MV photon beam in combination with GNPs of different sizes and it was inconsistent with previous radiobiological studies. The maximum DEF was achieved for 50nm GNPs in comparison with 30nm and 100nm leading to the assumption of self-absorption effect by larger diameters. According to the outcomes of this work, MAGICA polymer gel can be recommended as a reliable dosimeter to investigate the dosimetric effect of GNP size and also a useful method to validate the current radiobiological and simulation studies.

Keywords

Gold Nanoparticle, Polymer Gel, Dosimetry, Radiotherapy

Introduction

Radiotherapy is an important method for the treatment of cancer and nearly 50% of cancer patients receive radiotherapy during their treatment [1]. However, the presence of resistant cells to radiation is the cause of most failure and tumor relapse. Radiation sensitizers are agents that enhance the sensitivity of tumor cells to radiation

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damages. Recently, there has been a considerable increase in studying high Z (atomic number) nanomaterials mainly gold ($Z=79$), as a radiosensitizer [2]. The unique properties of gold have caused it to be suggested as the best candidate in nanoparticle radiotherapy. Radiobiological studies, including in-vivo and in-vitro researches, along with MC simulations have focused on investigating the effective sensitizing factors such as the nanoparticle size, concentration, surface features, radiation energy and cell type which can help to optimize the effect and possible clinical application of GNPs in radiation therapy [2-5]. Potential dose enhancement in kilovoltage (KV) radiation, is well-known and has been confirmed by many studies. However, since clinically, MV radiation is used for the most of the radiotherapy practices rather than KV energies, a much wider clinical application could be achieved if GNP radiosensitization was obtained using MV sources [6-7]. While the majority of studies have reported low or no increases in MV energies, there are some differences between biological and physical achievements using high energy clinical beams [6], which make it necessary to improve the measurement methods for studying GNP application in radiotherapy. Another considerable factor is GNP size that may play an important role in both radiation toxicity and sensitization [8-9]. While most researches have been performed investigating the smaller (less than 2nm) GNPs, 50nm GNPs have shown a better radiosensitization effect [10]. However, size has been reported to be a less relevant factor in sensitization by some studies verifying both large (up to 100nm) and small (2nm) diameters [11-12]. The differences between studies outcomes introduce some more investigations to help the current results coming into a close conclusion. Recently, using a polymer gel dosimeter impregnated with GNP has been suggested as a reliable method to perform the dosimetric investigation of GNP application in radiotherapy. Previous studies

considering beam energy and GNP concentration utilizing various polymer gels have been accomplished successfully [13-14]. Therefore, the dosimetric study of GNP using a tissue equivalent polymer gel would be a remarkable method to verify the current biological and simulation studies and also help to justify the applicability of GNP in clinical environments. This study uses MAGICA (Methacrylic Ascorbic in Gelatin Initiated by Copper with Agarose added) polymer gel as a radiation dosimeter to evaluate the effect of GNPs with large diameters (30, 50 and 100nm) on the macroscopic dose enhancement factor in MV radiation therapy.

Material and Methods

A. Gold nanoparticle

GNPs of 30nm, 50nm and 100nm size were purchased from PNF Co. (Tehran, Iran) in the form of aqueous solution with 0.5 mg/ml (500ppm) concentration. Nanoparticles size was determined using DLS (Malvern, UK) and TEM (Philips, 30M-10, Netherlands). Figure 1 shows the TEM images of GNPs.

B. Gel fabrication

The MAGICA polymer gel used in this study was prepared using Fong et al. [15] method with a little different due to adding agarose. First, the water was divided into five flasks to dissolve each material. About 60% of the total HPLC de-ionized water was used in gelatin and left in the room temperature to swell for about one hour. Two electrical heater-stirrer units were used to heat and solve the solutions. Gelatin was heated up to 50°C until a clear solution was obtained. About 30% of water which had been heated up to 70°C was used to dissolve the agarose, then heating and stirring continued up to about 90°C until all the agarose were solved. Then both gelatin and agarose solution were allowed to cool until about 47°C, at this time agarose solution was added to gelatin and stirring continued. Stirring never

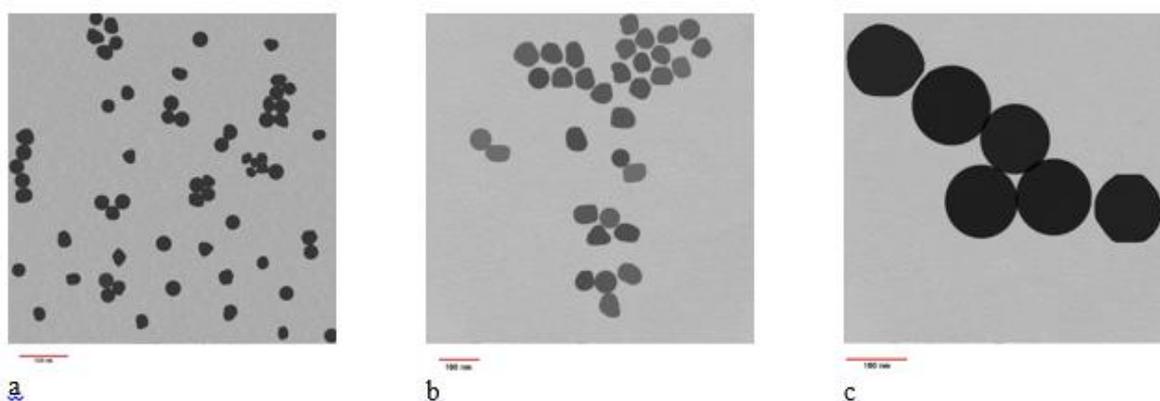


Figure 1: TEM images of GNPs a. 30nm GNP b. 50nm GNP and c. 100 nm GNP.

stopped before the end of fabrication. At 45°C hydroquinone, which had been solved in about 5% of water, was added to the mixture. The remaining 5% of water was divided into two portions for dissolving ascorbic acid and copper (II) sulphate. They were added to the mixture when the temperature was about 37°C. Methacrylic acid was added at the end [16]. When the preparation of MAGICA was completed, the solution separated into four portions, one part for MAGICA and three parts for incorporating GNPs with different sizes. According to previous works that achieved a maximum dose enhancement for this concentration, a constant concentration of 0.1mM was used in this study [13]. After preparation of MAGICA and Gold Nano-MAGICA (GN-MAGICA), they were poured in calibration tubes for being kept in the refrigerator at about 4°C.

C. Irradiation procedure

Gel samples were irradiated with 6MV photon beam from a medical linear accelerator (Siemens, Germany). The calibration tubes were set up in 50×50×50 cm³ water phantom at the Source to Surface Distance (SSD) =100 cm and field size of 30×30 cm² to cover all calibration tubes. They were exposed to radiation with specific doses in the range of 0-10 Gy (0, 2, 5, 7, 10 Gy). For verification of the MAGICA response of the 6MV x-ray beam, an

appropriate container of sizes 10×10×15 cm³ was made from plexiglass and irradiated with a field size of 10×10 cm² and SSD of 100 cm to obtain the PDD in the gel and then compare it with the TPS curve for the same irradiation condition, a single dose of 7Gy was applied.

D. MRI reading and processing

MRI was used to read out the polymer gel dosimeter. To ensure that the polymerization mechanism has completely done, 24 hours after irradiation all gel samples were scanned by a 1.5 T Philips (Achieva, Netherlands) MRI scanner using a head coil. A multi-spin echo sequence with 32 echoes, echo time of 15ms, repetition time of 3000ms, slice thickness 3mm and the field of view 300mm were used. Prior to the imaging process, samples were kept in the MRI room for about 4 hours to minimize the possible temperature gradient during imaging. R₂ maps were extracted from MR images using MATLAB software (version 8.4).

Results

MAGICA dose-response curve is shown in Figure 2 and represents a linear relationship between R₂ values and dose in the range of 0-10 Gy (with a good approximation of R²= 0.9812). Gel response of the 6MV X-ray beam was characterized by comparing the experi-

mental and TPS data of PDD curve which is shown in Figure 3. The Dose Difference (DD) was less than 4% for all points representing a good agreement between experimental and calculated data. DD curve is also presented in Figure 4.

The chemical interaction between gel and GNP must be take into account since it can interfere the dose measurement [17]. According to this the signals of non-irradiated tubes containing and not containing GNPs were evaluated and shown in Figure 5. Chemical interaction between GNPs with different sizes and MAGICA polymer gel could be ignored

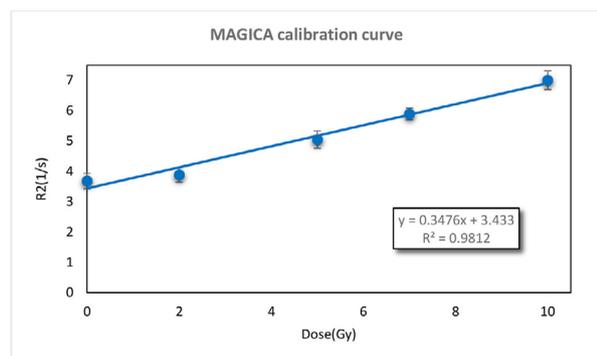


Figure 2: MAGICA calibration curve, presents a linear relation between R_2 and Dose ($R^2=0.995$).

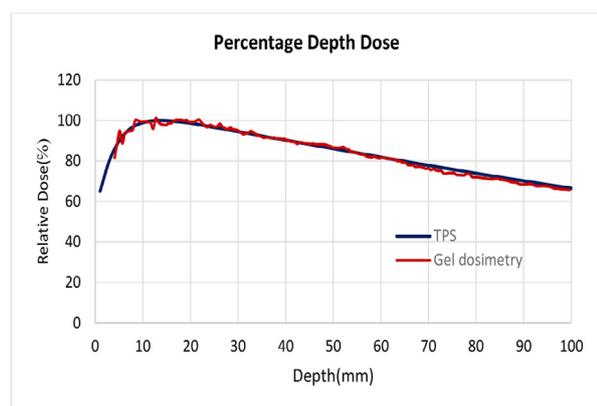


Figure 3: Comparison of PDD curves with gel dosimetry and TPS, DD for all points was less than 4% which shows a good agreement between experimental and TPS data.

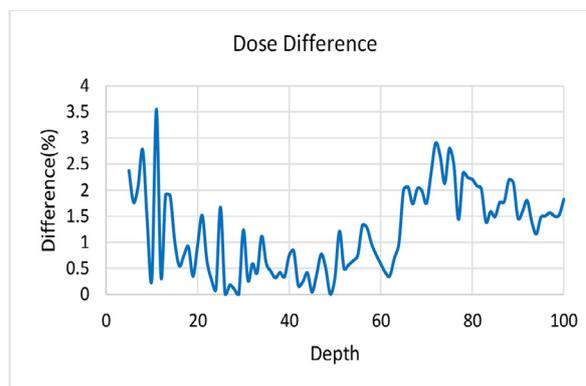


Figure 4: Dose Difference between MAGICA polymer gel dosimeter and Treatment Planning System (DD less than 4% for all points).

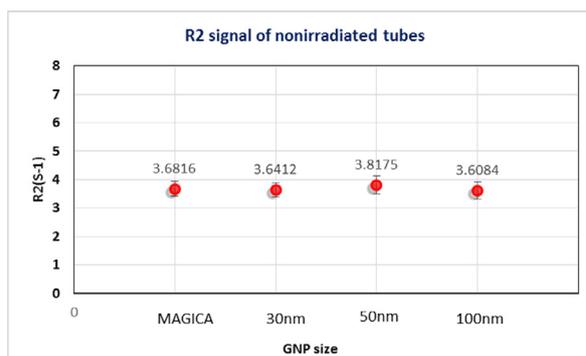


Figure 5: R_2 signal of non-irradiated tubes containing and not containing GNPs, R_2 signal variation less than 0.5%.

because of low R_2 signal variation (less than 0.5%).

The dose response curves for all the three GN-MAGICA samples containing 30nm, 50nm and 100nm GNPs were calculated as it was achieved for the pure MAGICA and the ratio of the slopes (known as the sensitivity) was taken as the dose Enhancement Factor (DEF). Figure 6 a, b and c are presenting the dose response curves. It can be seen that in the presence of GNPs with different sizes the linear relation between R_2 values and dose in the range of 0 to 10 Gy dose did not change.

According to Figure 6 a, b and c the increase in gel sensitivity due to the presence of GNPs with different sizes can be seen. Table 1 also

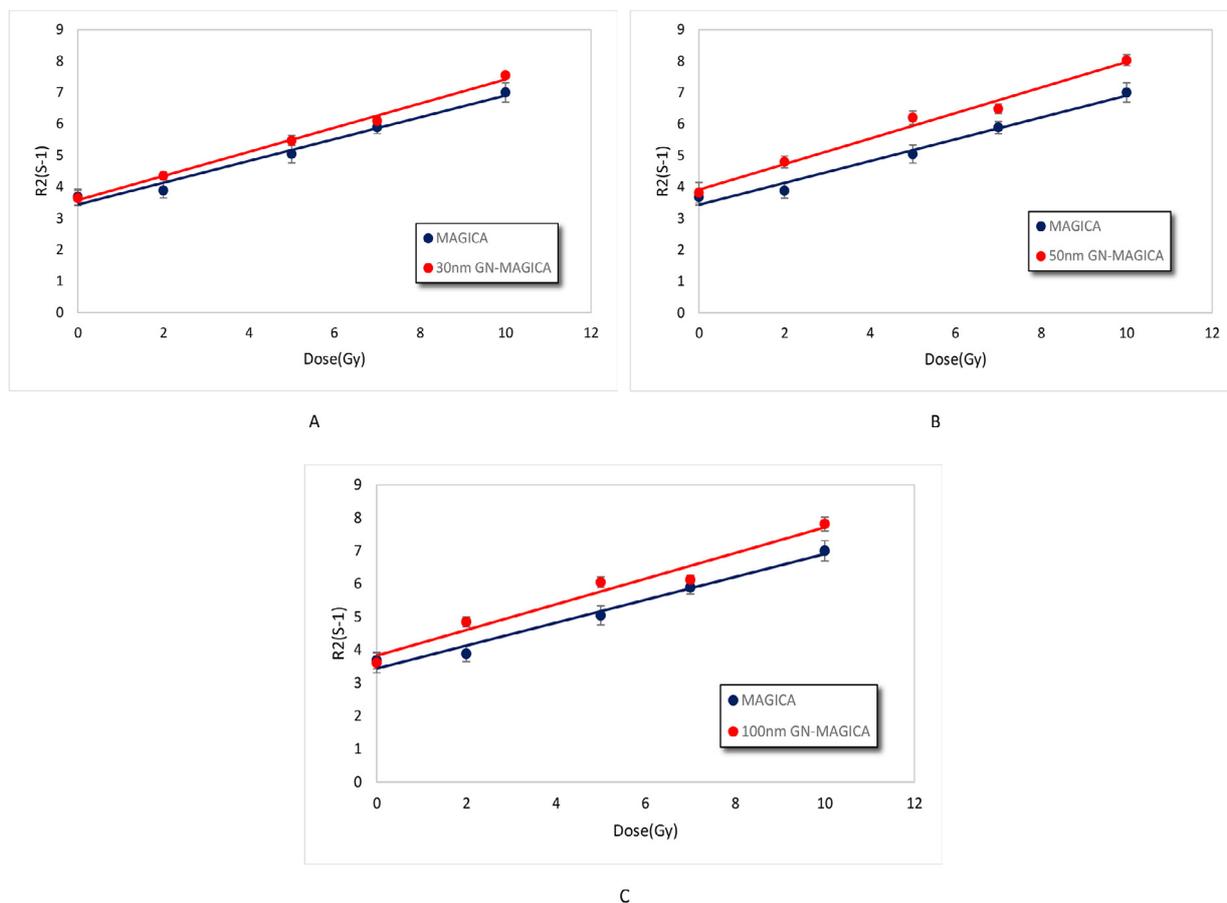


Figure 6: The dose response curves of GN-MAGICA samples with different sizes of GNP. (a) Dose response curve for 30nm GN-MAGICA, (b) dose response curve for 50nm GN-MAGICA and (c) dose response curve for 100nm GN-MAGICA. All curves show a linear relation in the range of 0 to 10 Gy.

summarizes the DEF and sensitivity of gel samples.

Achieved macroscopic DEFs for 30nm, 50nm and 100nm GNPs according to Table 1, are 1.1, 1.17 and 1.12, respectively. The 50nm GNP gain the maximum DEF in comparison with 30 and 100 nm GNP.

Discussion

The macroscopic DEFs due to the presence of 30nm, 50nm and 100nm GNPs using clinical 6MV photon beam were evaluated in this study and the DEFs of 1.1, 1.17 and 1.12 for 30, 50 and 100nm GNPs were achieved, respectively. The DEFs in this study, which are presented in Table 1, were derived from

Table 1: Representing the DEF achieved due to the presence of 30nm, 50nm and 100nm GNPs.

Gel Type	Sensitivity R-squared value	DEF
MAGICA	0.3476 S ⁻¹ Gy ⁻¹ R ² = 0.9812	
30nm GN-MAGICA	0.3838 S ⁻¹ Gy ⁻¹ R ² = 0.9944	1.1
50nm GN-MAGICA	0.4062 S ⁻¹ Gy ⁻¹ R ² = 0.9852	1.17
100nm GN-MAGICA	0.3889 S ⁻¹ Gy ⁻¹ R ² = 0.962	1.12

the ratio of the dose-response curve sensitivity of the GN-MAGICA and pure MAGICA polymer gel. The calibration curves of GN-MAGICA containing 30, 50 and 100nm GNPs in comparison with MAGICA are displayed in Figure 6 A to C, respectively. The mechanism underlying the increase in slope of dose-response curve is simply defined by the amount of polymerization occurring in the polymer gel. Under irradiation, radical species which are produced from the radiolysis of water initiate the polymerization in gel dosimeter. The extent of radiation-induced polymerization is a dose dependent and hence, it is expected that for a given dose, the gel dosimeter loaded with a radio sensitizer, undergoes a larger amount of polymerization due to the more radical generation. The degree of polymerization is then related to the spin-spin relaxation rate ($R_2=1/T_2$) measured by MRI [17-19]. Therefore, the R_2 -dose sensitivity will be higher for the polymer gel containing a radio sensitizer like GNPs. As it is presented in Table 1, the highest sensitivity develops for 50, 100 and 30nm GNPs, respectively which results to a maximum DEF for 50nm GNP. There is a comparable in-vitro study by Chitrani et al. [10]. Who investigated the radio sensitization effect of 14, 50 and 74nm GNPs in both KV and MV energies? In this study, 50nm GNP showed the highest sensitization effect and an enhancement factor of 1.17 was reported for 6MV photon beam which is inconsistent with our achievement. The author's discuss the difference in radio sensitization according to the number of GNPs internalized per cell since it was higher for 50nm GNP in spite of the same extracellular gold concentration. In our study also, 50nm GNP resulted in a larger amount of polymerization which then lead to a higher DEF in comparison with 30 and 100nm GNPs. Since the concentration was the same for all sizes, the most likely reason for small differences between DEF of 50 and 100nm GNPs, could be due to the self-absorption effect by a larger diameter. However, a

microscopic simulation study investigating 2, 50 and 100nm GNPs applying both KV and MV photon beams was carried out by Leung et al. [20], they came to the conclusion that self-absorption by particles can be ignored due to the larger portion of energy deposition outside the particles. It is also reported that GNPs with larger diameters lead to a greater dose enhancement due to the increase in total interaction number. Nevertheless, considering all components which were discussed in the article, including the effective range, deflection angle, radial dose distribution, energy and interaction processes of secondary electrons created during the interaction of photon beam with GNPs, the overall results may vary when multiple particles are present as in macroscopic studies, since in microscopic studies, just the manner of a single particle is investigated. In a macroscopic study by Mesbahi et al. and a nanodosimetric investigation by Lechman et al. considering the photon energy, nanoparticle size and concentration, size has shown to be a less relevant factor in dose enhancement and the number of photoelectric absorption for energies above the k-edge of gold atom [11-12]. They also have confirmed the effectiveness of GNP application in KV energies, while a negligible enhancement has been reported for MV energies. To discuss the differences between present and mentioned simulation studies, it is worth considering a recent study by McMahon et al [21] who calculated the nanodosimetric effect of a single GNP irradiated with MV energies. As a result of their investigation, a substantial dose in homogeneity was observed around the GNP that may contribute to the significant radio sensitization reported by some radiobiological studies in the range of MV energies. According to the cellular evaluation, it has been mentioned that GNPs tend to form large clusters up to hundreds of nanometers inside the vesicles. As GNPs get larger, their dose distribution properties become different from the smaller particles due to occurring a large portion of ionizing events within their

matter. This might be close to the assumption of self-absorption resulting a lower DEF in the case of 100nm GNP in comparison with 50nm particles in our study. On the other hand, in Leung et al. investigation, despite the more impressive application of GNPs in low energies, an interaction ratio of approximately 10 was achieved in higher energies that demonstrates an enhancement of secondary electron generation in the MV ranges [20]. This is in consistent with our study which presents a considerable dose enhancement for 6MV photon beam in combination with GNPs. Our result is also in close agreement with the study of Alqathami et al. [22] who used a novel multi compartment radiochromic radiation dosimeter to measure the dose enhancement produced by 50nm GNP irradiated with 100KV and 6MV x-ray beams. DEFs of 1.77 and 1.11 were obtained for KV and MV energies, respectively. A Close agreement between the outcomes of this article and previous studies would introduce the gel dosimeter as an appropriate method besides radiobiological and physical studies to find an accurate and optimal approach for the application of GNPs in radiotherapy

Conclusion

This article evaluated the macroscopic dose enhancement factor due to the presence of GNPs with different sizes in combination with 6MV clinical photon beam using MAGICA polymer gel dosimeter. The purpose of this study was to investigate the GNP size effect, mainly large sizes of 30, 50 and 100nm in the range of MV energies where low or no increases have been predicted by physical studies. Comparing the R_2 -dose sensitivity of GN-MAGICA and pure MAGICA, the DEFs of 1.1, 1.17 and 1.12 were achieved for 30, 50 and 100nm GNPs, respectively which shows for 50nm GNP, DEF was higher. It was assumed that the lower DEF of 100nm GNP in comparison with 50nm particles could be due to the self-absorption effect by larger diam-

eters. Our results were in a very close agreement with previous studies and this study introduces MAGICA polymer gel as a reliable dosimeter besides the radiobiological and simulation studies to achieve more accurate results for GNP application in radiotherapy.

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Conflict of Interest

None

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